Title:

Presymptomatic atrophy in autosomal dominant Alzheimer's disease: a serial MRI study

Authors:

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Abstract

INTRODUCTION: Identifying at what point atrophy rates first change in Alzheimer's disease is important for informing design of presymptomatic trials.

METHODS: Serial T1-weighed MRI scans of 94 participants (28 non-carriers, 66 carriers) from the Dominantly Inherited Alzheimer Network (DIAN) were used to measure brain, ventricular and hippocampal atrophy rates. For each structure, non-linear mixed effects models estimated the change-points when atrophy rates deviate from normal and the rates of change before and after this point.

RESULTS: Atrophy increased after the change-point, which occurred 1-1.5 years (assuming a single step change in atrophy rate) or 3-8 years (assuming gradual acceleration of atrophy) before expected symptom onset. At expected symptom onset, estimated atrophy rates were at least 3.6 times those before the change-point.

DISCUSSION: Atrophy rates are pathologically increased up to seven years before "expected onset". During this period, atrophy rates may be useful for inclusion and tracking of disease progression.

Keywords: Longitudinal, Atrophy, Alzheimer's disease, Dementia, Autosomal dominant, Neuroimaging, MRI, Boundary Shift Integral, Non-linear modeling, Change-point

1. Background

Testing potentially disease-modifying treatments for Alzheimer's disease (AD) during the preclinical phase [1] presents challenges of recruitment and staging of asymptomatic individuals, as well as determining suitable measures for assessing disease modification. One recruitment strategy is to study members of families known to carry a pathogenic mutation in a gene – *presenilin 1 (PSEN1), presenilin 2 (PSEN2) or amyloid precursor protein (APP)* – that causes autosomal dominant AD (ADAD). These mutations have almost 100% penetrance and ~50% of at-risk individuals are carriers. ADAD typically has an early and relatively predictable age at symptom onset [2,3]. The Dominantly Inherited Alzheimer Network (DIAN) is a multicentre observational study of individuals at risk of, or affected by, ADAD. DIAN performs longitudinal assessments of imaging, fluid biomarkers, and cognitive function, which reflect pathological features in ADAD [4] and sporadic AD [5]. In particular, cerebral atrophy measures derived from volumetric magnetic resonance imaging (MRI) are used as biomarkers of neurodegeneration and as outcome measures in trials [6].

Longitudinal data from presymptomatic ADAD individuals provide a unique opportunity to determine when atrophy rates begin to diverge from normal. Previous cross-sectional, or small longitudinal studies report a wide range of estimates of this point of divergence: from 10 years before [4,7] to 7 years after [8] expected clinical onset (as determined by the affected parent's age at onset).

Abbreviations: DIAN = Dominantly Inherited Alzheimer Network; ADAD = autosomal dominantly inherited familial AD; PSEN1 = presenilin 1; PSEN2 = presenilin 2; APP = amyloid precursor protein; EAO = expected age at onset; EYO = estimated years to expected symptom onset; NC = mutation non-carriers; pMut+ = presymptomatic mutation carriers; qMut+ = questionably or mildly symptomatic mutation carriers; sMut+ = overtly symptomatic mutation carriers.

We used serial MRI data from DIAN to model cerebral atrophy rates during presymptomatic and early symptomatic stages of ADAD. We assessed whole brain and hippocampal atrophy and ventricular expansion, three well-established imaging measures used as exploratory endpoints in clinical trials [6]. We hypothesize that presymptomatic carriers have similar atrophy rates to non-carriers up until a 'change-point' when the biomarker starts to diverge from normal. This hypothesis is consistent with models of sporadic AD [5] that assume a sigmoidal trajectory, and cross-sectional findings from the DIAN cohort [4,7]. We used two non-linear mixed effects models (Supplementary Appendix A) to estimate the timing of change-points relative to expected symptom onset, and atrophy rates before and after these change-points. The first model assumes that the atrophy rate undergoes a single 'step change' to a new, stable value; whereas the second model assumes a 'gradual acceleration' in atrophy rate after the change-point. These models help characterize when therapeutic effects on brain atrophy could potentially be observed in presymptomatic ADAD and could help focus future sample size calculations for upcoming prevention trials.

2. Methods

2.1 Participants and Procedures

All participants were members of DIAN [9], and details of participating sites are available (http://dian-info.org/). The study received prior approval from appropriate Institutional Review Boards and Ethics Committees at each site. Informed consent was obtained from all participants.

Genotyping was performed to determine the presence of an ADAD mutation for each at-risk participant. A semi-structured interview assessed the expected age at onset (EAO), based on when the affected parent first showed progressive cognitive decline. Expected years to symptom onset (EYO) is the difference between age at scan and EAO [3]. Negative values indicate years before expected onset and positive values years after.

At the sixth data freeze (July 2013), there were 102 participants with two or more MRI scans available and complete data (mutation status, age, EAO, and global Clinical Dementia Rating (CDR) score [10]).

2.2 Volumetric MRI

Volumetric T1-weighted scans were acquired on 3 Tesla MRI scanners using Alzheimer's Disease Neuroimaging Initiative (ADNI) standardized protocols [11] and corrected for intensity inhomogeneity [12]. Whole brain and hippocampal regions were automatically segmented [13–15]. Lateral ventricles were delineated semi-automatically by an expert rater. Baseline volumetric measures were corrected for total intracranial volume (TIV), calculated using an automated technique [16]. For each structure, volume change was directly measured using a group-wise implementation [17–19] of the Boundary Shift Integral (BSI) [20] to ensure longitudinal consistency. A trained image analyst, blinded to participants' mutation and clinical status, reviewed all raw and processed images.

2.3 Clinical Classification

Participants were classified into four groups, based on mutation status, global CDR score, and actual age at onset (where this had occurred), determined by Uniform Data Set form B9, “Clinical Judgment of symptoms” [21]:

- **Mutation non-carriers (NC);** our control group.
- **Presymptomatic mutation carriers (pMut+)**; included mutation carriers with a global CDR score of 0 at both their first two visits.
- **Questionably or mildly symptomatic mutation carriers (qMut+);** included participants with at least one global CDR score of 0.5 during their first two visits, with the other visit being either 0 or 0.5. We excluded from this group participants who had a reported onset more than four years before study entry.
- **Overtly symptomatic mutation carriers (sMut+)**; included participants with a CDR score of 1.0 or greater at either (or both) of their first two visits or who were more than four years after reported onset at study entry.

Eight participants were excluded from the analysis: seven (one NC, four pMut+, one qMut+, one sMut+) were identified during initial visual review of the image data and excluded due to non-Alzheimer’s pathology (e.g. infarct, neoplasm), imaging artifacts, or acquisition-related changes likely to result in unreliable atrophy measures. An additional participant (qMut+) was excluded due to moderate motion artefact on follow-up imaging and implausible growth in brain and hippocampi. As part of the sensitivity analysis, we re-ran the model including this participant (Supplementary Appendix B).

Two participants who initially satisfied the qMut+ criteria were retrospectively re-classified as sMut+, as both participants had consistent evidence of cognitive decline over a sustained period.

Our final sample therefore included 94 participants: 24 pMut+, 18 qMut+, 24 sMut+, and 28 NC. Of the 66 carriers, 54 had mutations in PSEN1, three in PSEN2, and nine in APP. There were 66 participants with two MR scans, 20 with three, and eight with four scans. The scan interval between baseline to follow-up ranged from 0.9 to 3.3 years, and was independent of carrier status or clinical severity. Two participants (one qMut+ and one sMut+) had inadequate image quality for analyses involving hippocampi.

2.4 Statistical analysis

To compare baseline values between each of the three mutations groups (pMut+, qMut+, sMut+) and the non-carrier group, ANOVA models were used for age, EYO, and TIV, while logistic regression was used for APOE $\varepsilon 4$ positivity and sex. A generalized least squares linear regression model that allows different group-specific residual variances was used to compare baseline volumes (standardized to mean TIV) between each of the three carrier groups and non-carriers.

The change-point model [22–24] was used to explore brain, ventricular and hippocampal atrophy rates (Supplementary Appendix A provides a detailed model description). As the focus of our study was the presymptomatic and earliest symptomatic stages of ADAD, the model included non-carriers (NC), presymptomatic, and questionably symptomatic carriers (pMut+/qMut+).

Figure 1 provides a schematic representation of the ‘step change’ and ‘gradual acceleration’ change-point models. In both, β represents the shared atrophy rate for NC and pMut+/qMut+ groups before the change-point, which takes place δ years before or after the EAO. Due to limited data, δ (for a specific brain structure) was assumed to be the same for all pMut+/qMut+ individuals.

For the ‘step change’ model, γ is the change in atrophy rate for the pMut+/qMut+ group after the change-point. In the ‘gradual acceleration’ model, the atrophy rate for the pMut+/qMut+ group accelerates after the change-point by a value of 2γ per year. With each model, we estimated β, γ and δ for each region, and using these we estimated atrophy rates at various points before and after EAO.

Our change-point model was not designed to estimate atrophy rates several years after symptom onset; to do so risked distorting a model that was designed to focus on the progression from early changes to clinical symptoms. Thus, a separate linear mixed-effects random-slopes model (with no change-point) was used to model atrophy rates of the sMut+ group, assuming all observations were after the change-point.

The change-point models are non-linear extensions of a previously described linear mixed-effects random-slopes model [25] (Supplementary Appendix A). Atrophy measures were log-transformed to provide symmetric approximations of percentage change from baseline. The change-point models were implemented using SAS

(version 9.4) procedure NLMIXED, which simultaneously estimated β, γ and δ. Robust estimates of uncertainty for these coefficients were obtained through bootstrapping [26,27], with 10,000 replicates and using bias corrected and accelerated (BCa) 95% confidence intervals. Sensitivity of the estimates and confidence intervals to outliers was explored (see Supplementary Appendix B).

3. Results

Table 1 summarizes demographic and clinical data. The sMut+ group was, as expected, older than the non-carriers, with smaller brain and hippocampal volumes, and larger ventricular volumes (all TIV-adjusted), reflecting pathological losses and larger TIV, which likely reflects the higher (albeit statistically non-significant) proportion of males in this group. The qMut+ group had smaller hippocampal volumes and larger ventricular volumes compared to non-carriers, while the preMut+ group just had smaller right hippocampal volumes.

Table 2 shows the change-point model results for each structure. In the 'step change' model, the pre-change atrophy rate (β) was statistically significant in every structure except the right hippocampus. In all regions, there were significant increases in atrophy rate (γ) after the change-point. This is demonstrated by deriving, from the results of the model, a ratio between the atrophy rate at EAO (1-0 years before) to the pre-change atrophy rate. This ratio was 4.0 for whole brain, 4.5 for ventricles, and 9.0 for left hippocampus, but it could not be produced for right hippocampus as the estimated pre-change atrophy rate was small and not statistically significantly different from zero. However, the increase in atrophy rate (γ) after the change-point for the right hippocampus was larger than the corresponding

coefficient in the results for the left hippocampus. The estimated change-point (δ) for brain, ventricle and left hippocampus was 1.4 years before EAO and 1.1 years before EAO for the right hippocampus. For whole brain and left hippocampus, the confidence intervals for δ did not span zero, providing evidence that they occurred before EAO. Estimates of the ventricular change-point had greater uncertainty (−1.1 to 13.5 years) than the other structures. Table 2 provides estimates for rates of change at various times before and after EAO.

As with the 'step change' model, in the 'gradual acceleration' model all structures except the right hippocampus had statistically significant pre-change atrophy rates. All regions had coefficients (γ) indicating statistically significant increased neurodegeneration after the change-point. The ratio of atrophy rate at EAO to the pre-change rate was 3.6 for whole brain, 4.1 for ventricles, and 5.1 for left hippocampus. The ratio for the right hippocampus was also not available due to the small, non-significant pre-change atrophy rate, but the coefficient (γ) indicated that the right hippocampus had a similar increase towards neurodegeneration as the left. The change-point estimates (δ) for the whole brain and ventricles were 3.0-4.6 years earlier than for the hippocampi. For all structures, the confidence intervals for δ did not span zero. Figure 2 shows estimated atrophy rates and 95% confidence intervals from both models in relation to EYO.

In the sensitivity analysis, we re-ran the model including the participant with movement artefact and clinically implausible data (Supplementary Appendix B). The pattern of the results was not materially altered although the statistical significance of some parameter estimates was lost.

The estimated rates of change in sMut+ participants were approximately double those found in pMut+/qMut+ carriers at EAO using the change-point models. The symptomatic rates were: −2.41% (95% CI: −2.88, −1.95) per year for whole brain, 15.0% (95% CI: 12.6,17.5) for ventricles, −4.70% (95% CI: −6.39, −3.01) for left hippocampus, and −4.64% (95% CI: −5.68, −3.60) for right hippocampus.

4. Discussion

The goal of this study was to estimate when brain, ventricular and hippocampal volume changes in ADAD diverge from non-carriers, and to model the rates before and after this transition using serial MRI data from the DIAN cohort. We designed two non-linear mixed effects models: one assuming a single ‘step-change’ and another assuming a ‘gradual acceleration’ in rates of atrophy after the change-point. This type of model has previously been used to investigate the trajectories of cognitive decline [23,28] and atrophy rates [29,30]. In all cases, there was evidence of increased atrophy after the change-point, suggesting that our models better reflect the non-linear nature of atrophy in early-stage disease than a linear relationship would. The 'gradual acceleration' model found evidence for all assessed regions that atrophy rates diverge from normal values before symptom onset, with the change-point occurring 3.0 to 7.6 years before EAO. The ‘step change’ model found a change-point of 1.4 years before EAO for whole brain and left hippocampus but was unable to show evidence of a change-point preceding EAO for ventricles or right hippocampus.

4.1 Interpreting the change-point model results

A key advantage of using two different change-point models is that they provide complementary information about the timing of the change-point. The 'step change' model provides the most conservative estimate of when atrophy rates diverge. In contrast, the 'gradual acceleration' model is probably more biologically plausible, based on previous results in ADAD [4,7,31,32] and by the well-characterised spatial spread of neurodegeneration [33] that typically begins in the medial temporal lobe and gradually spreads into neocortical regions. However, there are caveats to the gradual acceleration model used. The non-linear nature of the atrophy may vary between individuals and a quadratic may not be the most appropriate fit. However, given the size of the dataset, this approach minimizes risk of overfittings. Change-point models also avoid some of the pitfalls that can occur when including polynomial terms in a linear regression to model this non-linear relationship [34]. While a quadratic term could better capture the increase in atrophy rate observed around expected onset, it may also produce artefacts of increased atrophy in carriers who are decades before their expected onset.

Unlike linear models, change-point models can capture the different phases of atrophy/expansion during the long period of presymptomatic disease progression. Both models provide similar estimates of β (see Table 2), the pre-change atrophy rate. This suggested age-related changes broadly consistent with previous aging studies [35–37] showing small but significant rates of whole-brain atrophy of the order of 0.2-0.6%/year and hippocampal atrophy of the order of 0.3-0.4%/year for similar age ranges to this cohort. From both models, there was evidence of increased atrophy after the change-point in all regions.

4.2 Estimating onset of pathological atrophy

It is unclear when disease-related atrophy first becomes evident in ADAD. Cross-sectional results from *PSEN1* E280A mutation carriers [38,39] and DIAN [4,7] suggest atrophy of hippocampi diverge from non-carriers ~6 years and 10 years before symptom onset, respectively; earlier than in our models. However, initial longitudinal results from DIAN [7] (N=53) identified increased atrophy rates only in symptomatic carriers. A study of 13 presymptomatic *PSEN1* carriers found increased cortical thickness at baseline but subsequent thinning of a number of cortical regions [40], suggesting a non-linear nature to presymptomatic changes – with grey matter increases preceding declines.

Most previous longitudinal volumetric MRI studies of ADAD mutation carriers have been relatively small, single-site studies. One study following presymptomatic participants to clinical onset indicated pathological hippocampal atrophy rates appeared ~5.5 years before AD diagnosis [31]. Weston et al. [41] examined cortical thickness longitudinally in presymptomatic carriers and detected significant losses in the precuneus eight years before EAO. These values are consistent with our findings using a gradual acceleration model where the change point was 7.6 years before onset. However, another study of 16 ADAD mutation carriers (seven with long-term follow-up) did not detect structural MRI changes until *after* symptom onset [8], suggesting that a heterogeneity in these small cohorts and the methods used to analyze them may generate markedly different results.

No prior ADAD study has used change-point models, making it difficult to compare estimates. However, there are similarities between our findings and sporadic AD

studies that used similar approaches. A study of 79 elderly patients, 37 of whom developed mild cognitive impairment (MCI), reported a ventricular expansion change-point 2.3 years before MCI diagnosis [29]. Another longitudinal study (N=296, 66 progressing to MCI) found a similar hippocampal atrophy change-point of 2-4 years before clinical onset [30]. Their estimate of a 0.2% per year pre-change hippocampal atrophy rate accords with ours (0.2% left, 0.1% right). Their post-change atrophy rate estimate for the right hippocampus (2.7%/year) was similar to our value (2.5%) whereas their left hippocampal rate estimate (1.2%) was lower than our (2.1%).

4.3 Predicting clinical onset in ADAD

An important challenge is what estimate to use for clinical onset before it has occurred. Many studies, including ours, use an EAO based on when the affected parent first developed symptoms consistent with progressive decline. Other measures are based on the average across all previously affected family members, or the reported age at onset in the literature for a particular mutation [3]. However, each is an imperfect estimate of the future age at onset.

If future clinical trials use EYO as an inclusion criterion, then it is the distribution of atrophy rates relative to EAO that is of importance. However, if we wish to understand the etiology of the disease, then the distribution of atrophy rates relative to actual onset is more informative, as change-points are likely to be more strongly related to actual rather than expected age at onset. The effect of switching from actual to expected onset in statistical models will change the form of the estimated volume change over time, smoothing it to some degree. Without knowledge of actual

onset, this effect is not easily avoided. We did, however, attempt to reduce its impact by excluding overtly symptomatic carriers from our change-point models.

Identifying precisely when clinical onset has occurred is not straightforward. To facilitate standardization across sites, DIAN rigorously monitors how raters perform CDR and other assessments [42]. In at-risk individuals, other factors can influence cognitive function or behavioral changes, including stress, anxiety, and the constant level of vigilance and introspection that participants experience. In this study, there were six qMut+ participants who reverted from a baseline global CDR of 0.5 to 0 at follow-up. These cases highlight the subtle nature of transitions from unimpaired to "affected" and the potential confounds of mood disturbance and other factors. We addressed this uncertainty by including questionably or mildly symptomatic carriers in our change-point models.

4.4 Limitations and future work

Change-point models have been used to model atrophy rates in preclinical sporadic AD [29,30]. We expand on these approaches by adapting the model for repeated measures of direct change instead of individual volumetric measures and allowing for either a 'step change' or 'gradual acceleration' after the change-point. Due to the non-linear nature of our models, and the use of bootstrapping to obtain confidence intervals for the model coefficients, these models are susceptible to influential outliers, especially with smaller sample sizes (see the sensitivity analysis in Supplementary Appendix B). Additional longitudinal data should provide improved robustness against such issues.

No prior study has characterized the progression of atrophy in such a large cohort of presymptomatic and earliest symptomatic ADAD. DIAN is currently recruiting participants into a multicentre clinical trial [43], and the samples from our analysis should more closely reflect a clinical trial setting. Whole brain, lateral ventricles, and hippocampi are the most studied structures in sporadic AD, and are often used as trial outcome measures. From the results, these atrophy measures appear to be elevated compared to non-carriers approximately 5 years before expected onset, making them best suited for prevention trials in ADAD from this period onward. Given the evidence of presymptomatic atrophy in specific cortical regions [40,41], future application of the change-point model could involve studying atrophy rates of specific cortical structures, such as the precuneus and posterior cingulate. Atrophy in these structures may appear earlier and thus be better suited for trials that target presymptomatic patients. In addition, the model should incorporate information from other biomarkers, including CSF amyloid and tau concentrations, to determine how markers of these pathologies affect the timing of the change-point. Finally, it is essential to understand which preclinical changes in ADAD generalize to sporadic AD, as differences in the structures preferentially affected appear to exist [44].

4.5 Conclusions

Atrophy rates increase in ADAD some years before expected symptom onset. Using two different change-point models, we can characterize when this change occurs. The ‘step-change’ model provides a minimum estimate, 1.4 years before expected onset. The ‘gradual acceleration’ model provides a more biologically plausible approach towards how atrophy rates diverge from normal, with brain atrophy rates showing pathological acceleration ~7.6 years before expected onset and

hippocampal rates changing ~3.0 years before expected onset. These models may help predict the time to clinical onset for presymptomatic individuals with increased atrophy and identify individuals for prevention trials.

Figure captions

Figure 1: **Schematic representation of the 'step change' (Figure 1a) and 'gradual acceleration' (Figure 1b) change-point models.**

Figure 2: **Rates of change estimated from the 'step change' and 'gradual acceleration' models, as a function of the estimated years from symptom onset (EYO) for the pMut+/qMut+ carriers.**

The figure shows the relationship between rate of annualized volume change (%) and EYO. 95% confidence intervals are included, computed from the bootstrap samples. While the schematics in Figure 1 display the decline in actual volume, these graphs represent the rate of change in volume. A horizontal line indicates the estimated atrophy rate (from the 'step change' model) for non-carriers and carriers before the change-point before any deviation from normal rates of change. Vertical dotted lines indicate the change-points for both the 'step change' and 'gradual acceleration' models. For periods that include the change-point, the estimated rate of atrophy is a weighted combination representing the transition from the pre-change-point atrophy to the post-change-point atrophy. Top left: whole brain; top right: lateral ventricles; bottom left: left hippocampus; bottom right: right hippocampus.

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